

Morphological optimization of prosthesis' finger for precision grasping

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Abstract. In this paper, we present the morphological optimization of our tendon driven under-actuated robotic hand prosthesis' finger, to improve precision grasping. The optimization process is performed with a black box optimizer that considers simultaneously kinematic and dynamic constraints. The kinematic is computed with the Denhavit-Hartenberg parameterization modified by Khalil and Kleinfinger and the dynamic is computed from the virtual displacements and the virtual works. All these constraints are considered as a fitness function to evaluate the best morphological configuration of the finger. This approach gives a way to introduce and improve soft and flexible considerations for the grasping robots such as hands and grippers. Theoretical and experimental results show that flexible links combined with morphological optimization, lead in more precise grasping. The results of the optimization, show us an important improvement related to size, torque and consequently energy consumption.

Key words: Morphological optimization, mechanisms prehension, precision grasping, soft robotic

1 Introduction

Frequently, robots are designed as rigid structures, but recently some works have shown that the use of flexible bodies, actuators, and sensors could improve considerably the performance of the robots to interact with the environment, this kind of robots is known as soft robots. Soft robotic [1] systems could be able to improve grasping and manipulation, because they use: (i) elastic and deformable bodies, (ii) unconventional materials (like smart materials, shape memory alloy [2], i.a.) and (iii) high number of degrees of freedom.

In this context, the University of Bologna developed the UB-HAND IV, also called DEXMART Hand [3]. The hand is based on an endoskeletal structure articulated via pin joints, the actuators are located remotely with tendon-based transmissions, it has a soft cover and the mechanical structure of the hand was manufactured using additive technologies [4].

With the aim of building a robust and safe hand the University of Pisa and the Advanced Robotics Department of the Italian Institute of Technology in Genoa pro-

posed the Pisa-IIT Soft Hand. This hand incorporated traditional and rolling contact joints with elastic ligaments. The rolling contact joints ensure a correct motion while the hand is actuated. In case of impacts, these joints provide an easy disengage and allow deformations. The hand has a single tendon, passing through all the joints simultaneously. The tendon produces flexion-extension and adduction-abduction of the fingers during the actuation [5].

Consequently, an important tool named Mooveit! [6] incorporates the latest advances in motion planning, manipulation, control and navigation of arms, grippers and hands i.a. Even if the tool is designed for rigid robots it constitutes an interesting approach.

The consideration of a tendon driven under-actuated mechanisms, flexible links and soft articulations in kinematics chains, introduces the necessity of optimal analysis of the morphological parameters. In this domain, one important development is presented by Jouandeau [7], which is related to "Enhancing Humanoids Walking Skills through Morphogenesis Evolution Method", in that work the optimization was performed using confident local optimization for noisy black-box parameter tuning (CLOP)[8].

Based on our first prototype, we observe that an optimization of the finger lengths is wide important to increase the precision and reduce the torque requirements. Consequently, considering that the target of our robotic hand is the precision grasping, we begin the design process with the optimization of the finger that is the key element of the robotic hand.

Therefore, in this paper we propose the application of CLOP to improve the performance of our tendon driven finger, during the precision grasping. Our approach is to use the mathematical model of the kinematic (based on the Denhavit-Hartenberg parameterization modified by Khalil and Kleinfinger) and dynamics (based on the virtual displacements and virtual works) as the fitness function to evaluate the best morphological configuration of the finger. This approach gives a way to introduce and improve soft and flexible considerations for the grasping robots such as hands and grippers.

2 Kinematic and dynamic modelling of the robotic hand prosthesis' finger

2.1 Description of the robotic hand prosthesis' finger

Our approach is a bio-inspired tendon-driven finger composed of three joints, the metacarpophalangeal (MP), the proximal interphalangeal (PIP) and the distal interphalangeal (DIP). The MP joint has two degrees of freedom (DoF); one rotation (to perform flexion-extension), and one passive translation that allows the vertical alignment of the joint with the motor axis. The PIP and DIP joints have one DoF to perform flexion and extension.

The finger is under-actuated, so it is controlled by only one servo motor. The drive mechanism uses two tendons for transmitting motion to the finger, one tendon flex the finger and the other extend the finger. Considering that the tendons are attached to the motor pulley and the fingertip, as shown in Fig. 1, the clockwise rotation of the servo motor causes a flexion, and the anticlockwise rotation produce an extension. Due to the under actuation the rotation angles of the PIP (θ_{35}) and DIP (θ_{36}) joints are linked with the rotation angle of MP (θ_{33}) joint. The relation between angle is given as $\theta_{35} = 0.23\theta_{33}$ and $\theta_{36} = 0.72\theta_{33}$, where θ_{33} is the MP joint angle, θ_{35} is the PIP joint angle and θ_{36} is the DIP joint angle.

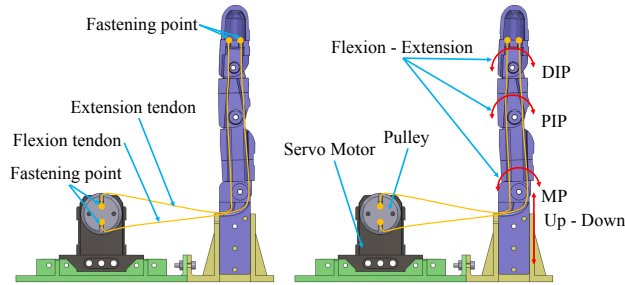


Fig. 1: Section view of the finger mechanism

The kinematic and the dynamic modeling are presented in the following subsections. For the kinematics, the Denhavit-Hartenberg parameterization modified by Khalil and Kleinfinger (DHKK) is used and for the dynamics we use the virtual displacements and virtual works approach. The equivalent mechanical model of the finger is shown in Fig. 2a for the kinematic and in Fig. 2b for the dynamic.

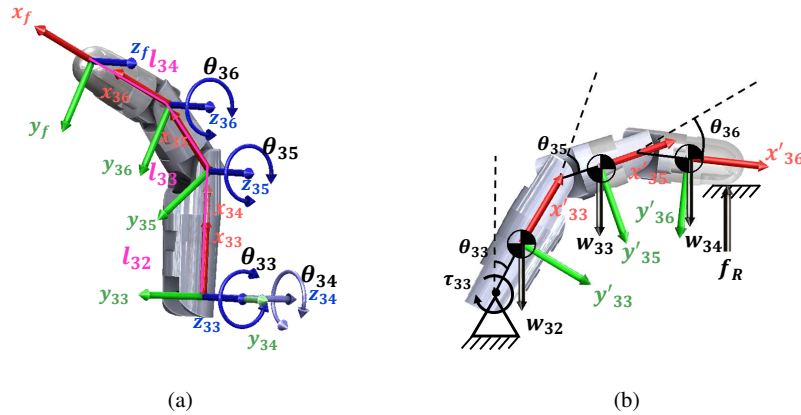


Fig. 2: Equivalent models of the finger. (a) Kinematic Model. (b) Dynamic model

In Fig. 2a, the parameters l_{32} , l_{33} and l_{34} are the lengths of the proximal, medial and distal phalanges respectively. The angles θ_{33} , θ_{34} , θ_{35} and θ_{36} correspond to MP, PIP and DIP joints rotations. The frameworks (x_{33}, y_{33}, z_{33}) and (x_{34}, y_{34}, z_{34}) are associated to the MP joint. The framework (x_{35}, y_{35}, z_{35}) is associated to the PIP joint and the framework (x_{36}, y_{36}, z_{36}) associated to the DIP joint. The framework (x_f, y_f, z_f) corresponds to the fingertip position. In the same way, in Fig. 2b, w_{32} , w_{33} and w_{34} are the weights of the proximal, medial and distal phalanges respectively, and are placed in the points (x'_{33}, y'_{33}) , (x'_{35}, y'_{35}) and (x'_{36}, y'_{36}) . F_r is the applied force that is equivalent to the reaction force.

2.2 Kinematic model of the robotic hand prosthesis' finger

To propose a method to model the kinematic of our robotic hand prosthesis' finger, we use the DHKK. This convention, allows the representation of open-loop and close-loop kinematic chains, and presents a convenient definition of:

- The rotation axis \mathbf{z}_i of each i -th joint
- The angle of rotation θ_i around \mathbf{z}_i
- The rotation α_i around \mathbf{x}_{i-1}
- The distance a_i along of \mathbf{x}_{i-1}
- The distance d_i along of \mathbf{z}_i

These parameters θ_i , α_i , a_i and d_i are known as DHKK parameters, and are calculated for each joint M_i with coordinates (x_i, y_i, z_i) , in Fig. 3 a graphical representation of these DHKK parameters is presented. The rotations are performed using the transformation matrix shown in Eq. (1)[9].

$${}^{i-1}T_i = \begin{bmatrix} \cos \theta_i & \sin \theta_i & 0 & a_i \\ \sin \theta_i \cos \alpha_i & \cos \theta_i \cos \alpha_i & \sin \alpha_i & \sin \alpha_i d_i \\ \sin \theta_i \sin \alpha_i & \cos \theta_i \sin \alpha_i & \cos \alpha_i & \cos \alpha_i d_i \\ 0 & 0 & 0 & 1 \end{bmatrix} \quad (1)$$

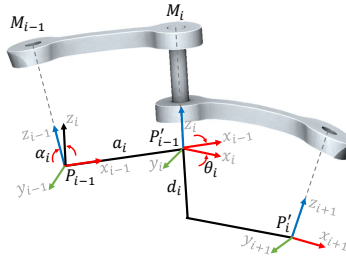


Fig. 3: Graphical representation of DHKK parameters

Consequently, the kinematics of a robot composed of n joints is the matrix 0T_n , which is a composition of the 3×3 orientation matrix 0R_n , and the position vector $[{}^0P_n^x, {}^0P_n^y, {}^0P_n^z]^T$, as shown in the following expression:

$${}^0T_n = \prod_{i=1}^n {}^{i-1}T_i = \left[\begin{array}{ccc|c} & & & {}^0P_n \\ \hline 0 & 0 & 0 & 1 \\ \hline \end{array} \right] \quad (2)$$

Usually, the formulation of DHKK parameters is difficult, because is performed manually, and is more difficult when there are multiple kinematic chains. Even that, a method to automatically generate these parameters is presented in [10], and is the adopted methodology to parameterize in the present work. The DHKK parameter for our finger are shown in Table 1, using the configuration shown in Fig. 2a.

Table 1: DHKK Parameters of the robotic hand prosthesis' finger.

Link	α_i	a_i	d_i	θ_i
33	$-\pi/2$	0	0	θ_{33}
34	$\pi/2$	0	0	θ_{34}
35	$-\pi/2$	l_{32}	0	θ_{35}
36	0	l_{33}	0	θ_{36}
f	0	l_{34}	0	0

Operating the Eq. (1) with the DHKK parameters of the robotic hand prosthesis' finger, shown in Table 1, we get a set of five matrices ${}^0T_{33}$, ${}^{33}T_{34}$, ${}^{34}T_{35}$, ${}^{35}T_{36}$ and ${}^{36}T_f$, that describe the transformation between the links of the kinematic chain. Applying the Eq. (2) with the calculated ${}^{i-1}T_i$ matrices, we get the position $[{}^0P_n^x, {}^0P_n^y, {}^0P_n^z]^T$ and orientation 0R_n of the joints.

Considering that the frameworks M_{33} and M_{34} are in the same position of the reference framework, the position vectors of ${}^0T_{33}$ and ${}^0T_{34}$ are zero (see Eq. (3), and Eq. (4)). From Eq. (3) to Eq. (7) we use the abbreviations $C_i := \cos(\theta_i)$ and $S_i := \sin(\theta_i)$.

$${}^0T_{33} = \left[\begin{array}{ccc|c} C_{33} & -S_{33} & 0 & 0 \\ \hline 0 & 0 & 1 & 0 \\ \hline -S_{33} & -C_{33} & 0 & 0 \\ \hline 0 & 0 & 0 & 1 \\ \hline \end{array} \right] \quad (3)$$

$${}^0T_{34} = \left[\begin{array}{ccc|c} C_{33}C_{34} & -C_{33}S_{34} & S_{33} & 0 \\ \hline S_{34} & C_{34} & 0 & 0 \\ \hline -C_{34}S_{33} & S_{33}S_{34} & C_{33} & 0 \\ \hline 0 & 0 & 0 & 1 \\ \hline \end{array} \right] \quad (4)$$

The following equation corresponds to the position $[{}^0P_{35}^x, {}^0P_{35}^y, {}^0P_{35}^z]^T$ and orientation ${}^0R_{35}$ of the joint M_{35} .

$${}^0T_{35} = \left[\begin{array}{ccc|c} C_{33}C_{34}C_{35} - S_{33}S_{35} & -C_{35}S_{33} - C_{33}C_{34}S_{35} & -C_{33}S_{34} & l_{32}C_{33}C_{34} \\ C_{35}S_{34} & -S_{34}S_{35} & C_{34} & l_{32}S_{34} \\ -C_{33}S_{35} - C_{34}C_{35}S_{33} & C_{34}S_{33}S_{35} - C_{33}C_{35} & S_{33}S_{34} & -l_{32}C_{34}S_{33} \\ \hline 0 & 0 & 0 & 1 \end{array} \right] \quad (5)$$

The following equation corresponds to the position $[{}^0P_{36}^x, {}^0P_{36}^y, {}^0P_{36}^z]^T$ and orientation ${}^0R_{36}$ of the joint M_{36} .

$${}^0T_{36} = \left[\begin{array}{ccc|c} {}^0r_{11} & {}^0r_{12} & C_{33}S_{34} & {}^0P_{36}^x \\ S_{34}(-S_{36}S_{35} + C_{36}C_{35}) & -S_{34}(S_{36}C_{35} + C_{36}S_{35}) & -C_{34} & {}^0P_{36}^y \\ {}^0r_{31} & {}^0r_{32} & -S_{33}S_{34} & {}^0P_{36}^z \\ \hline 0 & 0 & 0 & 1 \end{array} \right] \quad (6)$$

where

$$\begin{aligned} {}^0r_{11} &= C_{34}(-S_{36}S_{35} + C_{36}C_{35})C_{33} - S_{33}(S_{36}C_{35} + C_{36}S_{35}) \\ {}^0r_{12} &= -C_{34}(S_{36}C_{35} + C_{36}S_{35})C_{33} - S_{33}(-S_{36}S_{35} + C_{36}C_{35}) \\ {}^0r_{31} &= (-S_{36}C_{35} - C_{36}S_{35})C_{33} - C_{34}S_{33}(-S_{36}S_{35} + C_{36}C_{35}) \\ {}^0r_{32} &= (S_{36}S_{35} - C_{36}C_{35})C_{33} + C_{34}S_{33}(S_{36}C_{35} + C_{36}S_{35}) \\ {}^0P_{36}^x &= C_{34}(l_{32} + l_{33}C_{35})C_{33} - l_{33}S_{33}S_{35} \\ {}^0P_{36}^y &= S_{34}(l_{32} + l_{33}C_{35}) \\ {}^0P_{36}^z &= -S_{33}(l_{32} + l_{33}C_{35})C_{34} - l_{33}C_{33}S_{35} \end{aligned}$$

The following equation corresponds to the position $[{}^0P_f^x, {}^0P_f^y, {}^0P_f^z]^T$ and orientation 0R_f of the fingertip.

$${}^0T_f = \left[\begin{array}{ccc|c} {}^0r_{11} & {}^0r_{12} & -C_{33}S_{34} & {}^0P_f^x \\ S_{34}S_{35}S_{36} & -S_{34}(S_{36}C_{35} + C_{36}S_{35}) & C_{34} & {}^0P_f^y \\ {}^0r_{31} & {}^0r_{32} & S_{33}S_{34} & {}^0P_f^z \\ \hline 0 & 0 & 0 & 1 \end{array} \right] \quad (7)$$

where

$$\begin{aligned} {}^0r_{11} &= C_{34}(-S_{36}S_{35} + C_{36}C_{35})C_{33} - S_{33}(S_{36}C_{35} + C_{36}S_{35}) \\ {}^0r_{12} &= -C_{34}(S_{36}C_{35} + C_{36}S_{35})C_{33} - S_{33}(-S_{36}S_{35} + C_{36}C_{35}) \\ {}^0r_{31} &= (-S_{36}C_{35} - C_{36}S_{35})C_{33} - C_{34}S_{33}(-S_{36}S_{35} + C_{36}C_{35}) \\ {}^0r_{32} &= (S_{36}S_{35} - C_{36}C_{35})C_{33} + C_{34}S_{33}(S_{36}C_{35} + C_{36}S_{35}) \\ {}^0P_f^x &= ((l_{33} + l_{34}C_{36})C_{35} + l_{32} - l_{34}S_{36}S_{35})C_{34}C_{33} \\ &\quad - (C_{35}S_{36}l_{34} + S_{35}(l_{33} + l_{34}C_{36}))S_{33} \\ {}^0P_f^y &= ((l_{33} + l_{34}C_{36})C_{35} + l_{32} - l_{34}S_{36}S_{35})S_{34} \\ {}^0P_f^z &= -((l_{33} + l_{34}C_{36})C_{35} + l_{32} - l_{34}S_{36}S_{35})S_{33}C_{34} \\ &\quad - C_{33}(C_{35}S_{36}l_{34} + S_{35}(l_{33} + l_{34}C_{36})) \end{aligned}$$

2.3 Dynamic model of the robotic hand prosthesis' finger

The proposed dynamic model uses the principle of the virtual displacements and virtual works [11]. We use the dynamic equilibrium to define a model of the input torque as function of the applied force. The virtual work δW is calculated for the external forces (e.g. weight, applied force and input torque) in Eq. (8) and the inertial forces (e.g. centrifugal forces) in Eq. (9).

$$\delta W_e = Q_e^T \delta r_e \quad (8)$$

where Q_e^T is the external forces vector and δr_e is the virtual displacement vector of the forces application points.

$$\delta W_i = M \ddot{q}^T \delta r_i \quad (9)$$

where M is the diagonal mass matrix composed of the masses m_i and inertias J_i , \ddot{q}^T is the acceleration vector and δr_i is the virtual displacement vector of the inertial frameworks.

The dynamic equilibrium is given by Eq. (10), but as in our model the rigid bodies have movements restrictions, the displacements in the points where forces are applied aren't independent, so to solve the equilibrium equation it is necessary separate the coordinates into dependent and independent coordinates.

$$\delta q^T [M \ddot{q} - Q_e] = 0 \quad (10)$$

In order to separate coordinates, the transformation shown in Eq. (11) is proposed, as result we have the equilibrium equation proposed in Eq. (12), which is separable.

$$\delta q = B \delta q_{ii}, B = \begin{bmatrix} -C_{qd}^{-1} C_{qi} \\ I \end{bmatrix} \quad (11)$$

where C_{qd} is the jacobian of dependent coordinates, C_{qi} is the jacobian of independent coordinates and I is the identity matrix.

$$\delta q_{ii}^T B^T [M \ddot{q} - Q_e] = 0 \quad (12)$$

Solving the equation Eq. (12), we obtain the dynamic function which give us the input torque τ_{33} as function of the force Fr and the kinematics q, \dot{q}, \ddot{q} . The resulting expression is shown in Eq. (13), where we use the abbreviations $C_i := \cos(\theta_i)$ and $S_i := \sin(\theta_i)$.

$$\tau_{33}(Fr, q, \dot{q}, \ddot{q}) = \frac{H_0 - 4l_{32}H_{12} + H_{13}(l_{33}S_{35} - 4)}{8l_{33}S_{35} - 32} \quad (13)$$

where $H_0 = 2l_{32}^2 \ddot{\theta}_{33} (l_{33} (m_{33} + m_{32}) S_{35} - 6m_{33} - 4m_{32}) (S_{33})^2$
 $H_1 = ((3\ddot{\theta}_{35} + \ddot{x}_{33}) m_{33} + 2\ddot{\theta}_{35} m_{34} + (m_{34} + 2m_{33} + m_{32}) g - 2Fr) l_{33} S_{35}$
 $H_2 = ((m_{33} + 2m_{34}) l_{33}^2 + 4m_{34} l_{33} l_{34} + 2m_{34} l_{34}^2)$

$$\begin{aligned}
H_3 &= ((1/2 m_{33} \ddot{y}_{33} + m_{34} \ddot{y}_{35}) l_{33} + l_{34} \ddot{y}_{35} m_{34}) C_{35} \\
H_4 &= 2 \ddot{\theta}_{36} S_{36} l_{34} m_{34} - 6 \ddot{x}_{33} m_{33} + 2 J_{33} \ddot{\theta}_{35} - 4 \ddot{x}_{35} m_{34} \\
H_5 &= (-6 m_{33} - 4 m_{32} - 4 m_{34}) g \\
H_6 &= 1/4 l_{32}^2 \ddot{\theta}_{33} (3/2 m_{33} + m_{32}) (C_{33})^2 \\
H_7 &= ((m_{33} + 2/3 m_{34}) l_{33} + 2/3 l_{34} m_{34}) \ddot{\theta}_{35} C_{35} \\
H_{11} &= 1/4 m_{33} l_{33} C_3 5 l_{32} C_3 3 \ddot{\theta}_{33} + 1/4 \ddot{\theta}_{35} H_2 C_{35}^2 \\
H_{12} &= (-1/2 m_{33} l_{33}^2 S_{35}^2 \ddot{\theta}_{35} + H_1 + H_{11} + H_3 + H_4 + H_5 + 8 Fr) S_{33} \\
H_{13} &= 8 (H_6 + 3/8 l_{32} (H_7 + 2 m_{33} \ddot{y}_{33} + 4/3 m_{34} \ddot{y}_{35}) C_{33} + J_{32} \ddot{\theta}_{33})
\end{aligned}$$

3 Finger prototype test platform set-up

With the aim of test the drive mechanism, we design a platform to carry out several experiments, the experiments seek to measure the kinematics of the finger and fingertip force using several servo motors. The platform permits to adjust the position of the MP joint with respect to the actuator axis, which guarantees that the actuator torque is transmitted to the tendons in the same condition. The CAD model of the test platform is shown in Fig. 4.

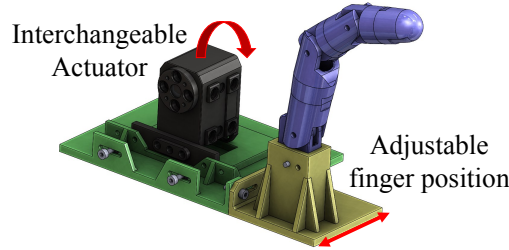


Fig. 4: CAD Model of the test platforms

3.1 Materials and methods

The experiments are performed using two standard servo motors HS-422 and Traxxas 2065 with torques of $0.324Nm$ and $0.225Nm$ respectively, and three serial servo motors Dynamixel XL-320, AX-12a and MX-106R with torques of $0.390Nm$, $1.50Nm$ and $10.0Nm$ respectively. To measure the force, we use a resistive-based force sensor Flexiforce®, that measure up to $5N$, connected to a circuit that uses an inverting operational amplifier arrangement to produce an analog output based on the sensor resistance, the output voltage is registered with a digital oscilloscope.

The sensor is calibrated in the range $0.6N$ to $4.8N$. The sensor is placed in a support (platform) which is located in the trajectory of the fingertip.

Considering that the finger performs flexion and extension in 2D, the kinematic is measured using a high-performance 4 megapixel CCD camera Prosilica GE-2040, to track black markers placed on the finger joints and the fingertip.

3.2 Kinematic tracking and force measure

As result of the test, shown in Fig. 5, which corresponds to the measure of the position of each M_i joint (using the Traxxas 2065 servo motor), it is possible to identify several peaks, i.e. the ${}^0P_f^x$ value shows a perturbation after contact. These overshoots are produced by different phenomena as friction forces and other external causes. The maximal force value is $2.82N$, (using the Traxxas 2065 servo motor) Fig. 6 shows the fingertip force f_r during three repetitions of flexion and extension.

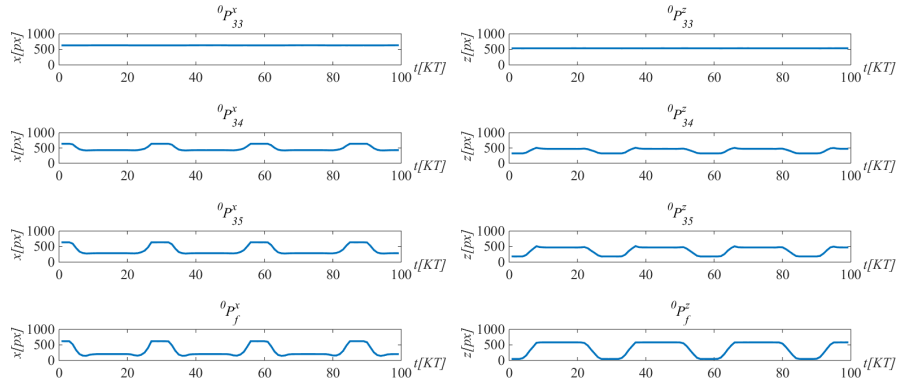


Fig. 5: Results of the position tracking using the Traxxas 2065 servo motor

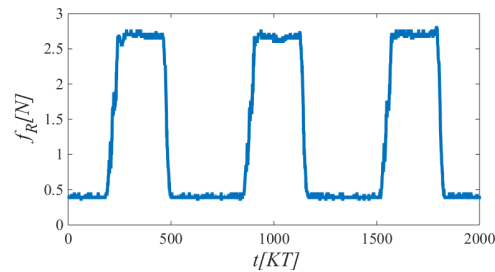


Fig. 6: Results of the fingertip force using the Traxxas 2065 servo motor

Although we cannot control external conditions, we identify that the performance of the finger is affected by the phalanges lengths. The lengths of the finger could increase the amount of torque needed to apply the same force over an object, and also may impact the precision of the grasping. So that, we propose a morphological optimization of the lengths of the finger phalanges, which is presented in Section 4.

4 Morphology optimization

This section introduces the proposed optimization process, which improves the movement of the finger during the precision grasping. This process seeks to find the optimal lengths of the finger phalanges, to reduce the position error during a grasping movement and also to reduce the torque τ_{33} to apply a force of $5N$.

The used method is confident local optimization (CLOP) for noisy black-box parameter tuning, which was developed to tune parameters in artificial intelligence for games. In our case, we follow the methodology proposed in [7] for enhancing the humanoids walking skills through morphogenesis evolution so that CLOP is implemented in two stages: evolution and evaluation.

4.1 Evolution process

The evolution process (based on an heuristic evaluation) uses as parameters the set \mathcal{H} (which contains Motors, Torques $\langle M, T \rangle$ and $lengths_{new}$ parameters, and their maximum and minimum values) and the eval function to calculate the fitness of the results. For each iteration, a new set of lengths is calculated and evaluated, the best result is updated when the founded solution is better than the stored one. The evolution process is presented in Alg. 1.

Algorithm 1 evolution $\langle M, T \rangle(n, \mathcal{H}, eval)$

```

1:  $(\mathcal{H}, \mathcal{L}) \leftarrow (\emptyset, \emptyset)$ ;
2: for  $i = 0$  to  $n$  do
3:    $lengths_{new} \leftarrow newParam \langle M, T \rangle(\mathcal{H})$ ;
4:    $(d, m) \leftarrow move(lengths_{new}, q_{initial}, q_{obj}, U, dt)$ ;
5:    $score \leftarrow eval(d, m)$ ;
6:   if  $score == ACCEPT$  then
7:      $insert((lengths_{new}, score), \mathcal{L})$ ;
8:   end if
9:    $insert((lengths_{new}, score), \mathcal{H})$ ;
10: end for
11: return best  $(\mathcal{L})$ ;

```

4.2 Evaluation process

The evaluation, use the results of the kinematic and the dynamic simulation to evaluate the fitness. The eval function determines two Euclidian distances: (i) distance d between the fingertip and the objective position (positioning error), and (ii) distance d_{best} between the best position founded and the objective position. Both distances are compared and the best result is updated only if d is lower than d_{best} . In the same way, the function analyses if the input torque m (which corresponds to τ_{33}) is lower than the best to modify the result. The eval function is presented in Alg. 2

Algorithm 2 eval (d, m)

```

1: if  $d < d_{best}$  then
2:    $(d_{best}, m_{best}) \leftarrow (d, m)$ ;
3:   return ACCEPT;
4: else if  $m \geq 0$  then
5:   if  $m < m_{best}$  then
6:      $(d_{best}, m_{best}) \leftarrow (d, m)$ ;
7:     return ACCEPT;
8:   end if
9: end if
10: return REJECT;

```

4.3 Experiment setting and application

To perform the experiment, two functions are defined, $f(lengths, q, u, dt)$ to describe the movement before the contact with the object to grasp and $g(lengths, x, u, dt)$ to describe the movement after the contact with the object.

Before contact, the parameter u is a speed control law defined as a ramp, which handle the engine speed to a maximal value with a constant slope. After contact u is a force control law that handles the applied force to a maximal value Fr with a constant slope. The algorithms to implement both functions are presented in Alg. 3 and Alg. 4.

Algorithm 3 kinematicMove ($lengths_{new}, q_{initial}, q_{obj}, U, dt$)

```

1:  $q \leftarrow q_{initial}$ ;
2:  $t \leftarrow 0$ ;
3: while contact ( $q$ ) == false do
4:    $(u, t) \leftarrow next(U, t, dt)$ ;
5:    $q \leftarrow f(lengths_{new}, q, u, dt)$ ;
6: end while
7: return (dist ( $q, q_{obj}$ ), -1);

```

Algorithm 4 DynamicMove ($lengths_{new}, x_{initial}, q_{obj}, Fr, U, dt$)

```

1:  $q \leftarrow \text{position}(x_{initial});$ 
2:  $x \leftarrow x_{initial};$ 
3:  $t \leftarrow 0;$ 
4: while contact( $q$ ) == false do
5:    $(u, t) \leftarrow \text{next}(U, t, dt);$ 
6:    $x \leftarrow g(lengths_{new}, x, u, dt);$ 
7:    $q \leftarrow \text{position}(x);$ 
8: end while
9: while torque( $x$ ) <  $Fr$  do
10:   $(u, t) \leftarrow \text{next}(U, t, dt);$ 
11:   $x \leftarrow g(lengths_{new}, x, u, dt);$ 
12: end while
13: return (dist( $q, q_{obj}$ ),  $u$ );
```

5 Results

The experiment, which was executed 150 times, search to minimize the position error and the torque τ_{33} . The evaluation process generates iteratively solutions, from the first (where l_{32} is 22.1mm and τ_{33} is 46Nmm) to the last (where l_{32} is 22.2mm and τ_{33} is 50.7Nmm). Each solution is equivalent or better than the previous. By applying the morphological optimization on l_{32}, l_{33}, l_{34} and τ_{33} parameters that produce f_R , we change parameters from (36.6mm 24mm 25mm 225Nmm) to (22.2mm 9.2mm 10mm 50.7Nmm) that improves f_R by a factor of 2 with a single finger experiment. Such gain over output force on each finger will be more important with a prosthetic hand with multiple fingers.

Table 2: Seven best results of the CLOP experiments.

$l_{32}[mm]$	$l_{33}[mm]$	$l_{34}[mm]$	$\tau_{33}[Nmm]$
22.1	19.6	16	46
26.5	15.3	13.3	58.6
26.2	10	18.9	55.1
23.1	12.9	10.6	52.3
22.9	12.8	10.3	51.8
18.9	9.9	13.1	40.3
22.2	9.2	10	50.7

The complete experiment, corresponding to the last row of Table. 2, is shown in Fig. 7a, where is possible to follow the evolution of the phalanges lengths and the trajectory described from the initial position to the objective position. Consequently, the result shows a direct relationship between the length of the phalange l_{32} and the

torque τ_{33} , and as can be shown in the Fig. 7b, the values are converging around a mean value.

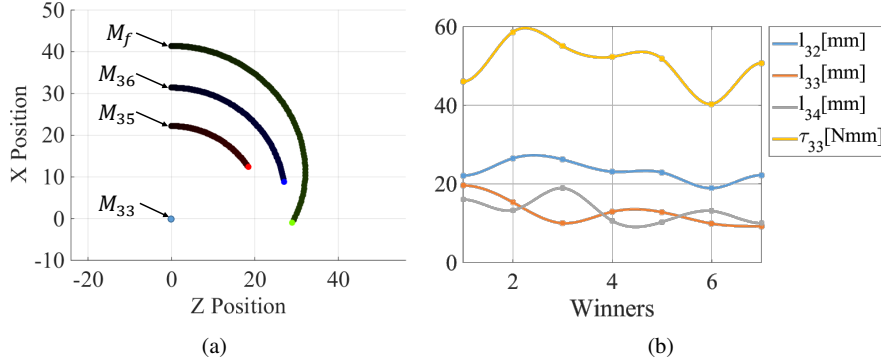


Fig. 7: Equivalent models of the finger. (a) Kinematic Model. (b) Dynamic model

6 Perspectives

The consideration of a tendon driven under-actuated mechanisms, introduces the necessity of torque control after the contact with the object to grasp, which in our case is the result of the optimal analysis of the morphological parameters. The morphological optimization performed, leads us to envisage a new finger, which should involve soft and flexible considerations for the design of the links and articulations, in order to achieve the grasping task in a more appropriate way. The results of the optimization, show us an important improvement related to size, torque and consequently energy consumption. Therefore, the next stage will be the integration of the optimal finger. Further investigations should also be tested to improve usability of robotic hand prosthesis with soft and flexible components.

7 Conclusions

The CLOP optimizer is a performant method that deals automatically with non-negative Hessians, which is the case of the proposed dynamic method. Consequently, the morphological optimal values allow to propose an evolution of our robotic finger. The obtained results show a smooth trajectory that is important for precision grasping. A similar optimization process could be applied to create an adaptive torque control grasping system.

The results of the performed torque optimization, give us an energetic performance, which render the robotic finger ideal to be used in our hand prosthesis. This energetic performance also lets the robotic hand prosthesis be more convenient to the patient according to the fact that we reduce the weight and increase the autonomy of the robot.

Acknowledgements Through this acknowledgement, we express our sincere gratitude to the Université Paris Lumières UPL for the financial support through the project PROMAIN This work has been partly supported by Université Paris Lumières UPL and by a Short Term Scientific Mission funding from LEME-UPO-EA4416 / LIASD-UP8-EA4383. We also acknowledge Colciencias - Colombia and the Universidad Militar Nueva Granada for the financial support of the PhD students.

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